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Regional and temporal heterogeneity of postsystolic wall thickening is associated with left ventricular asynchrony in normal and experimental stunned myocardium.

by

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ABSTRACT

Aims: Postsystolic wall thickening (PSWT) occurs after aortic valve closure. We investigated the influence of ischemia location and wall interactions on PSWT in normal and stunned myocardium.

Methods and Results: 22 dogs were studied. Seven chronically instrumented dogs (sonomicrometry) underwent 10-min coronary artery occlusion (CAO) of left circumflex artery (“LCX stunning”) and 7 other dogs underwent 10-min CAO of the anterior descending artery (“LAD stunning”) followed by reperfusion. At baseline, there was no PSWT in the anterior wall whereas posterior wall started and finished to thicken after the anterior wall, demonstrating PSWT. With LCX stunning, PSWT was observed in the posterior wall without affecting the remote anterior wall. With LAD stunning, PSWT in the anterior wall was transient and of lower magnitude vs posterior wall; in the remote posterior wall, PSWT previously observed at baseline, almost vanished. Postsystolic to systolic wall thickening ratio identified (ROC analysis) normal, ischemic and stunned myocardium with different amplitudes between walls. Tissue Doppler Imaging demonstrated similar pattern in basal, mid and apical segments (additional n=4 for both LCX and LAD stunning).

Conclusion: The present study demonstrates that location of ischemia and wall interactions produce discrepancies in PSWT between anterior and posterior walls in stunned myocardium.

KEYWORDS

Myocardial stunning

Regional function

Systole

Postsystolic wall thickening

INTRODUCTION

Postsystolic wall thickening (PSWT) is a part of the left ventricular thickening that occurs after aortic valve closure [1-3, 6, 8, 14-16, 18, 19, 22, 30, 32, 34, 35] and is a marker of left ventricular asynchrony [5] which has been extensively described during experimental [1, 2, 10, 13, 15, 16, 20, 29, 35, 36] and clinical [12, 14, 39] myocardial ischemia. The mechanisms involved in this phenomenon remain however still unclear and depend on the level of wall thickening and/or ischemic substrate [28]. Whether it is a passive recoil of the elastic myocardium and/or an active delayed contraction is still under debate [30].

Measurement of postsystolic wall motion has been proposed as a tool to assess the viability, to predict the recovery of left ventricular function during ischemic episodes and to evaluate the improvement of systolic performance during cardiac resynchronization therapy [2, 12, 29, 31, 35]. This issue is still debated and the presence of PSWT might not be an invariable marker of segment viability during ischemia and may not be always considered as pathognomonic of myocardial disease [34]. Part of this debate might result from regional heterogeneity as postsystolic wall motion is observed in approximately one-third of myocardial segments in healthy subjects [1, 39]. Posterior and anterior walls are indeed submitted to different stretching stresses and their extent and timing of thickening are therefore different [24, 41, 42]. To date, most of the studies investigated postsystolic wall motion while ischemia was produced either at the level of the anterior [4, 27-30, 35, 36] or the posterior [15, 16, 33] walls but to our knowledge, they had not been compared in the same experimental setting. Our hypothesis was that part of the confusion surrounding PSWT is the consequence of different experimental settings among the studies. Indeed, the locations of the ischemia and of the investigated stunned segment within the left ventricle are of major importance.

The goal of this study was thus to investigate the influence of ischemia location and wall interactions on the significance of PSWT in the normal and stunned myocardium. The evolution of PSWT was measured at baseline, during brief ischemia and subsequent stunning of either left ventricular anterior or posterior walls measured in the ischemic and the remote non ischemic zones. For this purpose, we performed occlusions of either the left anterior descending (LAD) or the left circumflex (LCX) coronary arteries in conscious dogs chronically instrumented with sonomicrometry. This model allows reproducible and repeatable measurements of regional myocardial thickening without interference with anesthetic agents [37]. Moreover, as instrumentation with multiple ultrasonic crystals is rather difficult (*e.g.*, apical, mid or basal within anterior and posterior walls), additional experiments in conscious state were performed using Tissue Doppler Imaging [40].

METHODS

The animal instrumentation and the experiments were performed in accordance with the official regulations of the French Ministry of Agriculture.

Instrumentation

As previously described [25], a left thoracotomy was performed in dogs (18 – 25 kg) and fluid-filled Tygon catheters were placed in the descending thoracic aorta as well as the left atrium for measurement of blood pressure. A solid-state pressure transducer (P7A, Konigsberg Instruments; Pasadena, CA, USA) was introduced into the apex of the left ventricle (LV). Pneumatic occluders were placed around the left circumflex coronary artery (LCX) and the left anterior descending coronary artery (LAD) at 2-3 cm from its origin. Two pairs of ultrasonic crystals were used for measurement of LV wall thickening in the distribution of LCX (posterior wall, so-called inferior wall in humans) and LAD (anterior wall) vascular beds. One crystal was implanted within the endocardium and the other was sutured to the epicardium in the mid region of the left ventricle. Proper alignment of the crystals was ensured by visualizing the signal on an oscilloscope. The pericardium was sutured after implanting the crystals. All catheters and wires were exteriorized between the scapulae and the pneumothorax was evacuated. Cefazolin (1 g *iv*) and gentamicin (40 mg *iv*) were administered before and during the first week after surgery. Post-operative analgesia was provided with morphine. The correct position of the crystals was verified at autopsy.

Hemodynamic measurements

All hemodynamic data were recorded and analyzed using the data acquisition software HEM v3.5 (Notocord Systems, Croissy sur Seine, France). Aortic and left atrial pressures were measured with a Statham P23 ID strain-gauge transducer (Gould-Nicolet, Courtaboeuf, France). LV pressure was measured using the Konigsberg gauge and the change in LV pressure over time (LV dP/dt) was computed from the LV pressure signal. LV pressure was calibrated *in vitro* with a mercury manometer and *in vivo* with the left atrial and aortic pressures. External electrocardiogram was also recorded.

Measurements of regional contraction

Wall thicknesses were obtained by using an ultrasonic transit-time dimension gauge (Module 201, System 6, Triton Technology Inc., San Diego, CA, USA). To determine wall thickening, end-diastolic wall thickness was measured at the initiation of the upstroke of LV pressure tracing and the end-systolic wall thickness was measured 20 ms before peak negative LV dP/dt [35].

As illustrated in Figure 1, systolic wall thickening was defined as the difference between end-diastolic and end-systolic wall thicknesses, *i.e.*, the wall thickening (expressed in % vs end-diastolic wall thickness) that occurs during the ejection period [9].

Maximal wall thickness was defined as the maximal distance between crystals, measured after aortic valve closure. Postsystolic wall thickening was defined as the maximal minus end-systolic wall thicknesses, *i.e.*, the wall thickening that occurs after the ejection period.

Minimal early systolic wall thickness was defined as the minimal distance between crystals measured after end diastole during the ejection period. Early systolic thinning was defined as the end-diastolic minus minimal early systolic wall thicknesses.

The time to onset of wall thickening (T_{onset}) was calculated as the time elapsed between end-diastole and the minimal early systolic wall thickness. Asynchrony of thickening between the posterior and the anterior walls was evaluated by $\Delta_{\text{onset}} = T_{\text{onset}} [\text{posterior wall}] - T_{\text{onset}} [\text{anterior wall}]$.

Measurement of regional myocardial blood flows

Regional myocardial blood flows were measured by the fluorescent microspheres techniques, as previously reported [26]. Microspheres labeled with fluorescent dyes (FluoSpheres, Triton System, San Diego, CA) were injected via the left atrial catheter. Arterial blood reference samples were withdrawn (7.5 ml/min during 2 min).

At termination of the study, the hearts were excised. The anatomical boundaries of the previously ischemic and nonischemic vascular beds were defined by dual perfusion of dyes in the left main coronary artery which was perfused with a solution of 3% Evans blue. The previously occluded circumflex or left anterior descending arteries were simultaneously perfused with saline. The heart was then cut into slices. Pictures were taken and the area at risk, *i.e.*, the non blue zone, was quantified by image analysis.

The slices were further divided into subendocardium, midmyocardium and subepicardium layers. Samples were processed to extract the fluorescence, and blood flows (expressed as

ml/min/g of myocardium) were calculated. Mean transmural flow was calculated as the combined flow of all three layers.

Tissue Doppler Imaging

An ultrasound system (Vivid 7, General Electric Medical System, Waukesha, WI, USA) and a 5-MHz phased-array transducer were used to analyse regional velocity of basal, mid and apical segments of the anterior and the posterior wall. Three beats of cardiac cycles in sinus rhythm were acquired to assess radial function. End-diastole and end-systole were first detected using aortic Doppler signal which was used to trigger the electrocardiogram. Timing of end-systole and end-diastole were then set according to the electrocardiogram.

Experimental protocol

Three weeks after instrumentation, when the dogs had fully recovered from their initial instrumentation, they were installed to lie quietly on a table in the conscious state. All animals received an injection of morphine sulfate (0.2 mg/kg SC) before coronary artery occlusion (CAO). After baseline measurements, a group of 7 dogs underwent a 10-min CAO of the LCX (so-called “LCX stunning” group) and a second group of 7 other dogs underwent a 10-min CAO of the LAD (so-called “LAD stunning” group). All hemodynamic and wall thickness parameters were continuously recorded and calculated at baseline, during CAO (9th min) and during the 6 hours of the subsequent reperfusion. Regional myocardial blood flows with the use of microspheres were measured during CAO (6th min). For Tissue Doppler Imaging purposes, two additional groups of animals (both n=4) underwent the same ischemia-reperfusion sequence. Echocardiographic measurements were performed at baseline and at 30 min of reperfusion.

Statistical Analysis

Data are reported as mean \pm S.E.M. Comparisons were performed using two-way ANOVA for repeated measures. If needed, only single individual comparisons between LAD stunning vs LCX stunning were conducted using Student *t*-test. Regression lines were calculated with the least-squares method. Receiver operating characteristics (ROCs) analysis were used to interpret values of postsystolic to systolic wall thickening ratio as well as postsystolic wall thickening in LCX stunning and LAD stunning. Sensitivity, specificity and area under curve (AUC) were calculated. A value of $p < 0.05$ was considered significant.

RESULTS

Hemodynamics

Representative recordings of hemodynamics, regional function by sonomicrometry and electrocardiogram are displayed in Figure 2. As shown in Table 1, heart rate, mean aortic pressure, LV pressure and LV dp/dt_{max} were not significantly different at baseline, during CAO and reperfusion between the two groups of dogs. Regional myocardial blood flows measured were similar during CAO between the LAD and LCX groups (0.08 ± 0.05 ml/min/g, n=4, and 0.10 ± 0.06 ml/min/g, n=5, respectively). Areas at risk were similar in both groups ($29 \pm 6\%$ and $31 \pm 4\%$, both n=7, respectively). As illustrated in Figure 2, there was no QRS prolongation during reperfusion.

Systolic wall thickening

Values of systolic wall thickening were not significantly different at baseline between the two groups (e.g., 27 ± 2 and 26 ± 3 % in the posterior wall for the LCX stunning group and in the anterior wall for the LAD stunning group, respectively). As illustrated in Figure 3, systolic wall thickening measured in the ischemic zone was severely depressed during CAO. During reperfusion, systolic wall thickening remained similarly depressed in the ischemic zones with both LCX and LAD stunning. In the remote non ischemic zone, systolic wall thickening remained unchanged with LCX or LAD stunning (Figure 3).

Postsystolic wall thickening

As illustrated in Figure 4, PSWT was observed at baseline in the posterior but not in the anterior wall. During CAO, PSWT in the ischemic zone was significantly greater after LCX vs LAD occlusions (13 ± 1 and 8 ± 2 %, respectively). As illustrated in Figure 4A, this difference was observed throughout the first hour of reperfusion.

In the remote non ischemic zone (Figure 4B), posterior PSWT decreased during LAD occlusion and early reperfusion (30 min) with LAD stunning. After that time-point, PSWT was again observed and tended to reach greater values as compared to baseline. In contrast, PSWT was not observed in the anterior wall at baseline and it remained not affected by LCX occlusion and subsequent stunning.

Asynchrony between the ischemic and the remote non ischemic zones: delayed wall thickening, early systolic wall thinning and postsystolic wall thickening

At baseline, there was a “physiological asynchrony” within the left ventricle: the posterior wall started to thicken after the anterior wall ($\Delta_{\text{onset}}=20\pm 5$ ms) and during this delay, wall thickening was replaced by a paradoxical early systolic wall thinning (0.10 ± 0.02 mm in the 14 dogs) (Figures 1 and 5). Posterior wall also finished to thicken after the anterior wall, *i.e.*, demonstrating PSWT (0.54 ± 0.15 mm in the 14 dogs). During myocardial stunning induced by LCX occlusion and reperfusion, the delay was increased as indicated by the arrow in Figure 5 (higher values of Δ_{onset}) and completion of PSWT was also delayed, *i.e.*, PSWT was increased. The overall timing in thickening of the non ischemic anterior wall was not affected by posterior wall stunning.

In the anterior wall, there was no delay in wall thickening at baseline and therefore no paradoxical early systolic wall thinning. During myocardial stunning induced by LAD occlusion and reperfusion, a delay in wall thickening was observed in the anterior wall during LAD stunning as indicated by the arrow in Figure 5 (negative values of Δ_{onset}). This delay was then accompanied by a paradoxical early systolic wall thinning and completion of anterior wall thickening was delayed, *i.e.*, PSWT was observed with LAD stunning. During LAD stunning, the “physiological asynchrony” of left ventricular walls was reversed: the posterior wall started to thicken without any delay before the anterior wall but it also finished to thicken before the anterior wall, *i.e.*, PSWT was not observed in the remote non ischemic posterior wall.

Importantly, the presence of a delay in wall thickening was always associated with an early systolic wall thinning and at that time, completion of wall thickening was also delayed, *i.e.*, there was PSWT. As illustrated in Figure 6, the evolution of PSWT in both zones was related to that of early systolic wall thinning with significant correlations between postsystolic wall thickening and early systolic wall thinning as well as between the duration of postsystolic wall thickening and the delay in wall thickening. Conversely, as illustrated in the anterior wall during LCX stunning, PSWT was not observed in the absence of a delay in wall thickening, *i.e.*, in the absence of systolic wall thinning.

Interpretation of postsystolic wall thickening

By ROC analysis, postsystolic to systolic wall thickening ratio was the best parameter to identify myocardial ischemia (cutoff: 1.7; sensitivity: 100%, specificity: 97%, AUC = 0.997, $p < 0.05$ in the anterior wall and cutoff: 1.1; sensitivity: 100%, specificity: 95%, AUC = 0.993, $p < 0.05$ in the posterior wall) as illustrated in Figure 6. Postsystolic to systolic wall thickening

ratio further allowed to distinguish between normal and stunned myocardium in the anterior wall (cutoff: 0.09; sensitivity: 53%; specificity: 100%; AUC = 0.802; $p < 0.05$) and in the posterior wall (cutoff: 0.3; sensitivity: 53%; specificity: 95%; AUC = 0.696; $p < 0.05$). ROCs analysis of the ratios showed that the cutoff values were lower for the anterior wall as compared to the posterior wall reflecting that the absolute value of PSWT was of higher amplitude.

Tissue Doppler Imaging

As illustrated in Figure 8, echocardiographic measurements demonstrated that at baseline, PSWT was a) absent in the anterior wall in basal, mid and apical segments and b) present in the posterior wall in basal, mid and apical segments. During stunning of the anterior wall (LAD stunning), postsystolic wall motion was observed in the mid and apical segments. Its absence in the basal segment was explained by the location of the occluder. At that time, postsystolic wall motion was no longer present in the remote posterior wall. During stunning of the posterior wall (LCX stunning), postsystolic wall motion was exacerbated in all segments as compared to baseline measurements; no postsystolic wall motion was observed in the remote anterior wall.

DISCUSSION

The present study investigated for the first time the consequences of anterior and posterior ischemia and subsequent stunning on postsystolic wall thickening measured simultaneously in the anterior and posterior ventricular walls. Postsystolic wall thickening was strikingly different between the anterior and the posterior walls. Despite the same pathophysiological context, postsystolic wall thickening was greater in the posterior than in the anterior wall as a result of the physiological (at baseline) or the pathological (at least with stunning) asynchrony and wall interactions within the left ventricle. Therefore, interpretation of postsystolic wall thickening should not only be analyzed along with systolic performance but it needs also to take into account the locations of regional ischemia and the considered segment (anterior *vs* posterior wall) as demonstrated by ROCs analyses.

Aynchrony and postsystolic wall thickening

We observed that in the normal heart, thickening of the posterior wall started later than in the anterior wall. This delay occurred during isovolumic contraction when LV pressure is rapidly increasing. During this time-period, one can speculate that the non-thickening posterior myocardium was stretched under pressure and normal thickening was replaced by a paradoxical early systolic wall thinning. During stunning of the posterior wall, both the delay in posterior wall thickening and early systolic wall thinning were increased. As shown by the increase in Δ_{onset} , myocardial stunning of the posterior wall exacerbated left ventricular asynchrony. This delay in the onset of thickening was accompanied by a prolongation of thickening after aortic valve closure, demonstrating PSWT. This relationship between the presence of PSWT and the delay of thickening at early systole, *i.e.*, the result of asynchrony, was further supported by the

correlation between PSWT and early systolic wall thinning. Interestingly, when posterior myocardial stunning declined, the asynchrony between anterior and posterior walls tended to return to baseline. In these conditions, Δ_{onset} , early systolic wall thinning and PSWT were simultaneously reduced. This delay in contraction observed in the posterior wall was not observed in a previous study investigating the consequences of LAD and LCX stunning. However, it should be stressed that these authors used an anesthetized open-chest model and a pericardial cradle which might have altered myocardial contraction [7].

If this relationship between ventricular asynchrony and PSWT described above is real, one can speculate that when there is no delay in wall thickening and when early systolic wall thinning tends to zero, PSWT should not be detected anymore. This is the case in our study as there was no delay for the anterior wall to thicken (early systolic wall thinning = 0 mm at baseline) and PSWT was not observed in this zone. This mechanism can also explain the behavior of PSWT during LAD stunning. Indeed, due to stunning, thickening of the anterior wall was delayed and Δ_{onset} became negative, *i.e.*, the posterior wall started to thicken before the anterior wall. In this situation, posterior thickening was not delayed anymore (T_{onset} and early systolic wall thinning close to 0) and posterior PSWT almost vanished during the first hour of anterior wall stunning. Conversely, thickening of the anterior wall was delayed and PSWT in the anterior zone was observed in these conditions. Such relationship between ischemia location within the left ventricle and the mechanical consequences have been previously reported during acute myocardial ischemia [11].

As discussed above, the presence of PSWT appears to result from a ventricular asynchrony. We did not attempt to distinguish between a passive recoil or an active contraction. On the one

hand, as myocardium is an elastic structure, PSWT might be the result of a restitution of early systolic thinning. On the other hand, it could also correspond to a delayed active contraction.

As one hallmark of myocardial ischemia was a depressed wall thickening during ejection, we further analyzed the significance of PSWT by also taking into account systolic wall thickening. Previous reports [19, 38] have performed similar analysis but they only proposed a single cut-off value for the entire ventricle without distinguishing anterior and posterior walls or taking into account the location of the ischemia. As illustrated in Figure 7, the present study demonstrated that cut-off values used to distinguish between the normal, ischemic and stunned myocardium are strikingly different between the anterior and the posterior wall. These values are much lower in the anterior wall as compared to the posterior wall. This demonstrates that PSWT might not be always considered as pathognomonic of myocardial dysfunction. Its clinical application would be improved by taking into account such heterogeneity. In addition, its measurement can provide interesting informations on the drugs effect on left ventricular function and wall interactions. For example, in a previous study, using this index, we have demonstrated that ivabradine, a pure heart rate reducing agent, converts the wasted postsystolic wall thickening into efficient ejectional wall thickening [23].

Our experimental model is well appropriate for studying regional wall thickening as all recordings were made in conscious animals, avoiding changes in loading conditions and the use of anesthetic agents [17] which are well known to interfere with myocardial performance [37]. Two segments were measured and analyzed in our study as compared to MRI [21, 42] but assessment of myocardial thickening during hours in stable conditions is not possible in anesthetized or open-chest models. Sonomicrometry crystals are long term implanted and the measure that they provide is highly reproducible whereas echocardiography can hardly provide

similar repetitive and reproducible measurements during hours. Nevertheless using Tissue Doppler Imaging, we demonstrated that the results obtained with sonomicrometry on mid segments were also observed in basal, mid and apical segments. Unfortunately due to an insufficient optimal positioning of the echocardiographic probe and a time consuming process, it was not possible to perform quantitative and repetitive Tissue Doppler Imaging measurements in the conscious dogs. The development of other echocardiographic approaches such as speckle tracking will probably solve in the future the limitations encountered in the present study.

In conclusion, the present study demonstrates that location of regional ischemia and wall interactions are responsible for great discrepancies in postsystolic wall motion between the anterior and posterior walls of the stunned myocardium.

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FIGURE LEGENDS

Figure 1

Typical waveform representing the evolution of myocardial wall thickness during a single beat recorded from a stunned posterior wall: (a) systolic wall thickening was defined as the difference between end-diastolic and end-systolic wall thicknesses; (b) maximal wall thickness was defined as the maximal distance between crystals measured after end-systole; postsystolic wall thickening was defined as the maximal minus end-systolic wall thicknesses; (c) minimal early systolic wall thickness was defined as the minimal distance between crystals measured after end-diastole. Early systolic wall thinning was defined as the end-diastolic minus minimal wall thicknesses; (d) the time to onset of wall thickening (T_{onset}) was calculated as the time elapsed between end-diastole and the early systolic minimal wall thickness. These measurements were performed using both sonomicrometry (left panel) and Tissue Doppler Imaging techniques (right panel; AVO : aortic valve opening; AVC : aortic valve closure).

Figure 2

Representative recordings of aortic blood and left ventricular pressures, left ventricular pressure first derivative (LV dP/dt), anterior wall thickness, posterior wall thickness and electrocardiogram measured at (a) baseline, (b) during a 10 min of left circumflex coronary artery occlusion (LCX CAO), (c) during myocardial stunning of the posterior wall after a 10-min coronary artery occlusion of the left circumflex coronary artery (LCX stunning), (d) during a 10 min of left anterior descending coronary artery occlusion (LAD CAO) and (e) during myocardial stunning of the anterior wall after a 10-min coronary artery occlusion of the left anterior descending coronary artery (LAD stunning).

Figure 3

Evolution of systolic wall thickening (% change from baseline) in the ischemic zone and remote non ischemic zone measured at baseline, during a 10-min coronary artery occlusion (CAO, 9th min recording) and reperfusion of the left anterior descending coronary artery (LAD stunning, $n=7$) and the left circumflex coronary artery (LCX stunning, $n=7$). The severities of myocardial stunning in the two zones were similar.

Figure 4

(A). Evolution of postsystolic wall thickening in the ischemic zone measured during a 10 min-period of coronary artery occlusion (CAO) and reperfusion of either the left anterior descending coronary artery (LAD stunning, $n=7$) or the left circumflex coronary artery (LCX stunning, $n=7$).

(B). Evolution of postsystolic wall thickening in the non ischemic zone measured during the 10-min CAO and reperfusion of either the left anterior descending coronary artery (LAD stunning, $n=7$) or the left circumflex coronary artery (LCX stunning, $n=7$). *, $p<0.05$ vs. LAD stunning.

Figure 5

Illustration of the asynchrony between the anterior and posterior walls at baseline and during myocardial stunning. At baseline, there was no delay in wall thickening in the anterior wall but posterior wall exhibited a delayed wall thickening as compared to anterior wall (as evaluated by Δ_{onset}), *i.e.*, posterior wall started to thicken after the anterior wall. This delay was characterized by two aspects: firstly, during this early systolic time-delay, the posterior wall paradoxically

thinned and secondly, wall thickening continued beyond end-systole, *i.e.* postsystolic wall thickening was observed.

During myocardial stunning induced by LCX occlusion and reperfusion (LCX stunning), the delay to thickening was increased as indicated by the arrow (increased positive Δ_{onset}) and both early systolic wall thinning and postsystolic wall thickening were exaggerated with LCX stunning (tracing recorded at 1h of reperfusion).

During myocardial stunning induced by LAD occlusion and reperfusion, as indicated by the arrow, a delay in wall thickening was observed in the anterior wall and was accompanied by a paradoxical early systolic wall thinning. Concomitantly, completion of anterior wall thickening was also delayed, *i.e.*, postsystolic wall thickening was observed. In this situation, Δ_{onset} was negative, *i.e.*, the posterior wall started to thicken without any delay before the anterior wall. Posterior wall also finished to thicken before the anterior wall, *i.e.*, postsystolic wall thickening was not observed anymore in the remote non ischemic posterior wall (tracing recorded at 1h of reperfusion).

Figure 6

A. Correlation between postsystolic wall thickening and early systolic wall thinning in the ischemic zones measured either in the left anterior descending coronary artery (LAD stunning, $n=7$, Postsystolic wall thickening = $1.35 \cdot \text{early systolic wall thinning} + 0.20$, $r = 0.69$, $p < 0.05$) or the left circumflex coronary artery (LCX stunning, $n=7$, Postsystolic wall thickening = $0.87 \cdot \text{early systolic wall thinning} + 0.45$, $r = 0.99$, $p < 0.05$).

B. Correlation between postsystolic wall thickening and early systolic wall thinning in the non ischemic remote zones measured either in the left anterior descending coronary artery (LAD stunning, $n=7$) or the left circumflex coronary artery (LCX stunning, $n=7$, Postsystolic wall thickening = $1.40 \times \text{early systolic wall thinning} + 0.31$, $r = 0.93$, $p < 0.05$).

C. Correlation between the duration of postsystolic wall thickening and the delay in wall thickening (Duration in postsystolic wall thickening = $0.14 \times \text{delay in wall thickening} + 61$, $r = 0.97$, $p < 0.05$).

Figure 7

Flow-chart of postsystolic wall thickening interpretation according to its location (anterior or posterior walls) and its amplitude in the normal, the ischemic and the stunned myocardium according to ROC analysis (Sens : sensitivity; Spec : specificity).

Figure 8

Representative tracings computed from Tissue Doppler Imaging recordings in basal, mid and apical segments of the anterior and posterior walls. Measurements were performed at baseline, in the stunned anterior wall (LAD stunning) and in the stunned posterior wall (LCX stunning). For each beat, the first and the second shaded lines represent aortic valve opening and closure, respectively.

Table 1. Hemodynamic measurements performed at baseline, during CAO and subsequent LAD stunning and LCX stunning sequences.

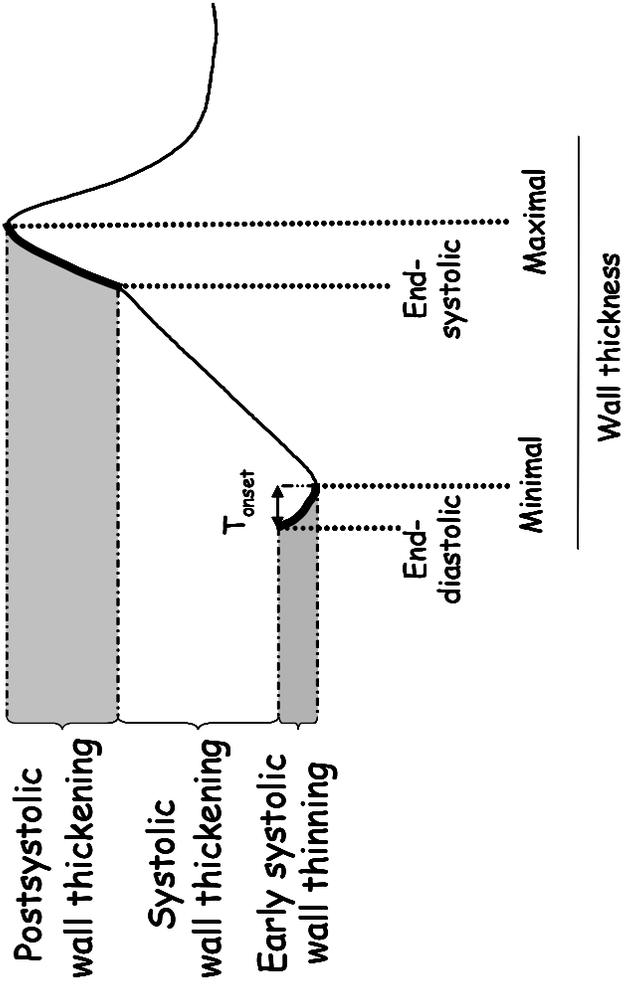
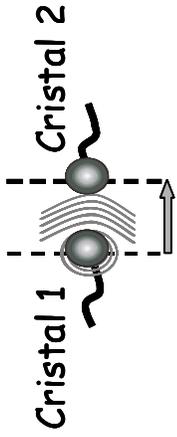
	Baseline	CAO	Recovery						
			15 min	30 min	1h	3h	6h		
HR, beats/min									
<i>LAD stunning</i>	81 ± 7	115 ± 8	80 ± 4	83 ± 6	78 ± 3	82 ± 4	78 ± 6		
<i>LCX stunning</i>	82 ± 7	118 ± 9	86 ± 7	81 ± 6	77 ± 8	80 ± 5	79 ± 4		
MAP, mmHg									
<i>LAD stunning</i>	96 ± 2	106 ± 8	98 ± 3	92 ± 5	90 ± 4	98 ± 4	92 ± 4		
<i>LCX stunning</i>	96 ± 4	102 ± 9	98 ± 3	96 ± 4	99 ± 4	95 ± 3	98 ± 4		
LV pressure, mmHg									
<i>LAD stunning</i>	128 ± 4	132 ± 8	127 ± 3	123 ± 4	124 ± 4	131 ± 2	127 ± 4		
<i>LCX stunning</i>	127 ± 4	129 ± 8	124 ± 6	126 ± 6	123 ± 7	132 ± 6	124 ± 6		
LVEDP, mmHg									
<i>LAD stunning</i>	7 ± 1	13 ± 3	9 ± 1	7 ± 1	6 ± 2	6 ± 1	7 ± 1		
<i>LCX stunning</i>	7 ± 1	13 ± 1	10 ± 2	9 ± 2	7 ± 2	7 ± 2	6 ± 1		
LV dP/dt _{max} , mmHg/s									
<i>LAD stunning</i>	3859 ± 287	3570 ± 219	3294 ± 189	3427 ± 208	3489 ± 219	3722 ± 287	3832 ± 300		
<i>LCX stunning</i>	3753 ± 273	3481 ± 327	3254 ± 169	3309 ± 266	3462 ± 212	3642 ± 308	3699 ± 276		
QRS duration, ms									
<i>LAD stunning</i>	49 ± 2	- -	51 ± 2	50 ± 1	49 ± 1	51 ± 1	50 ± 1		
<i>LCX stunning</i>	50 ± 2	- -	53 ± 1	52 ± 1	51 ± 1	50 ± 2	51 ± 2		

Values are means ± S.E.M., $n = 7$ dogs in both stunning sequences.

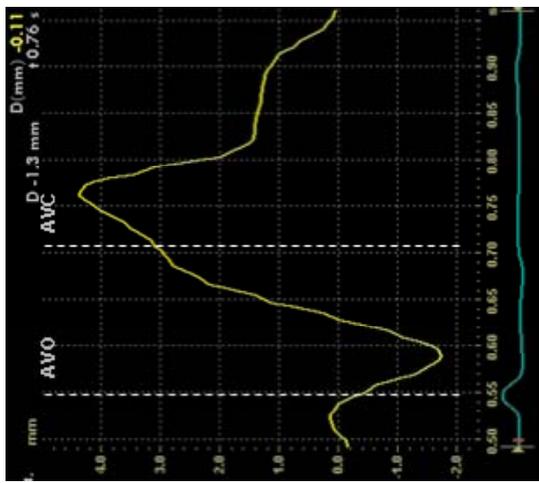
CAO, coronary artery occlusion; HR, heart rate; MAP, mean arterial pressure; LV: left ventricle; LVEDP: left ventricular end-diastolic pressure; LV dP/dt_{max}, maximum change in left ventricular pressure over time.

FIGURE 1

Sonomicrometry



Tissue Doppler Imaging



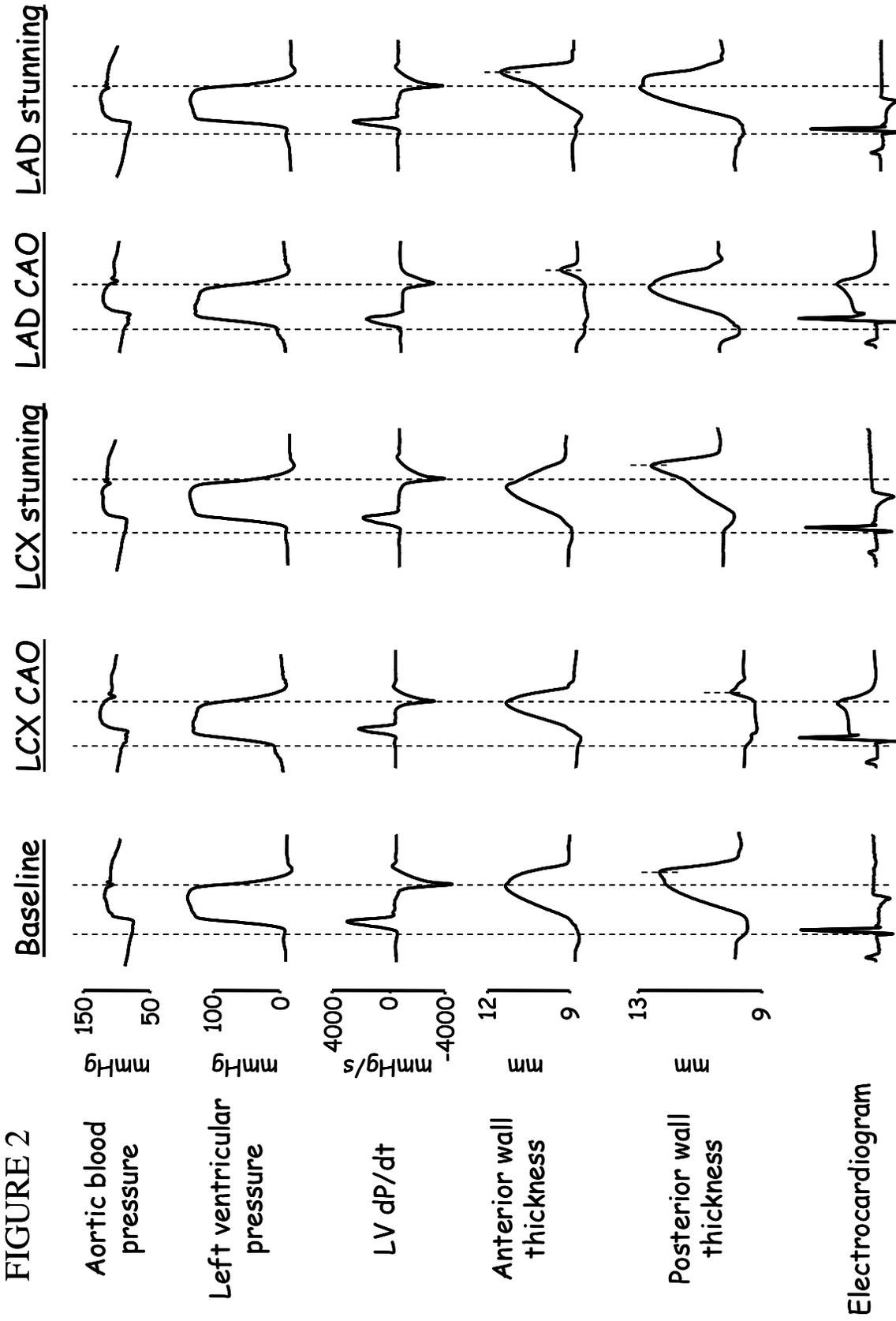
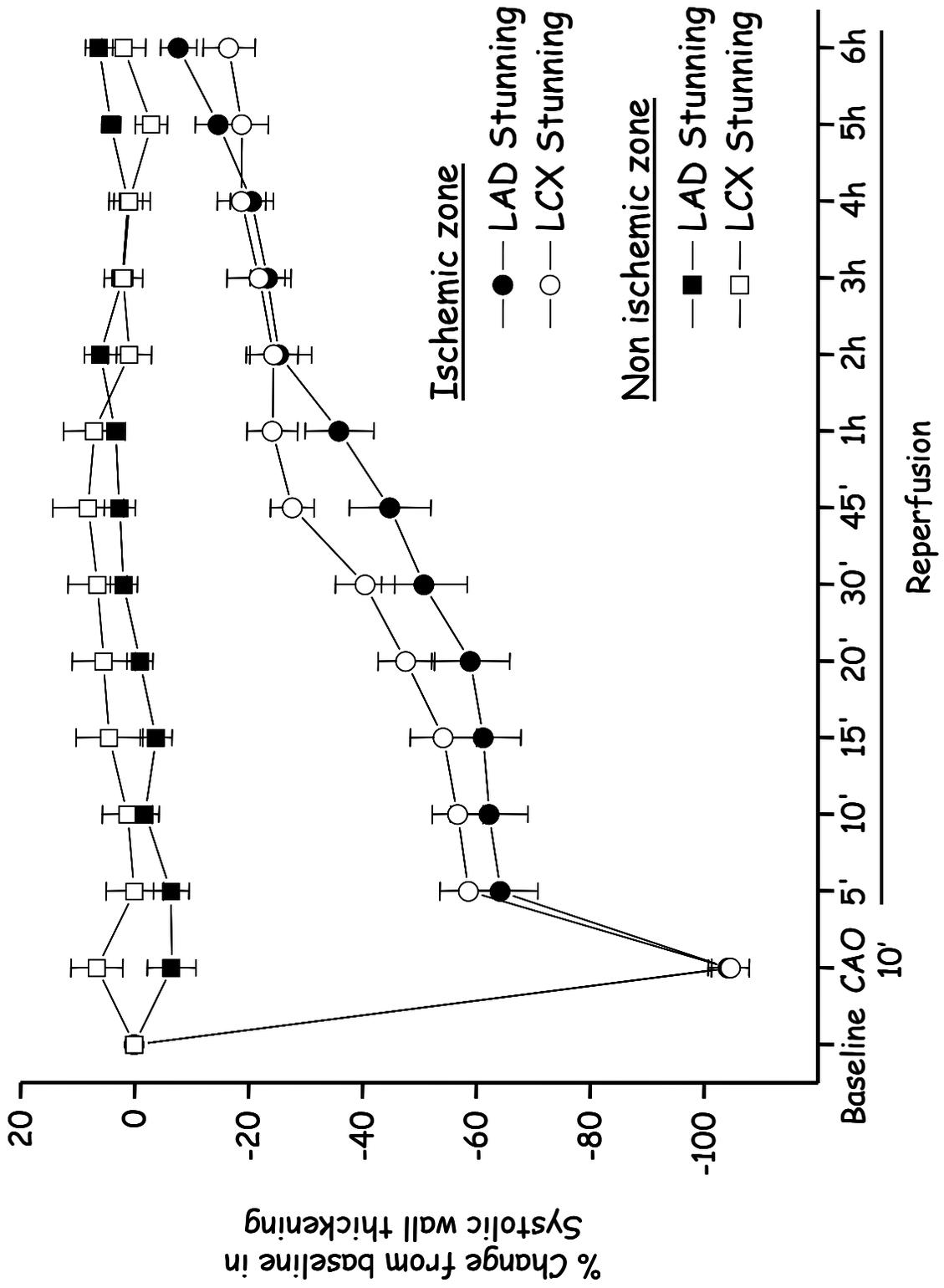
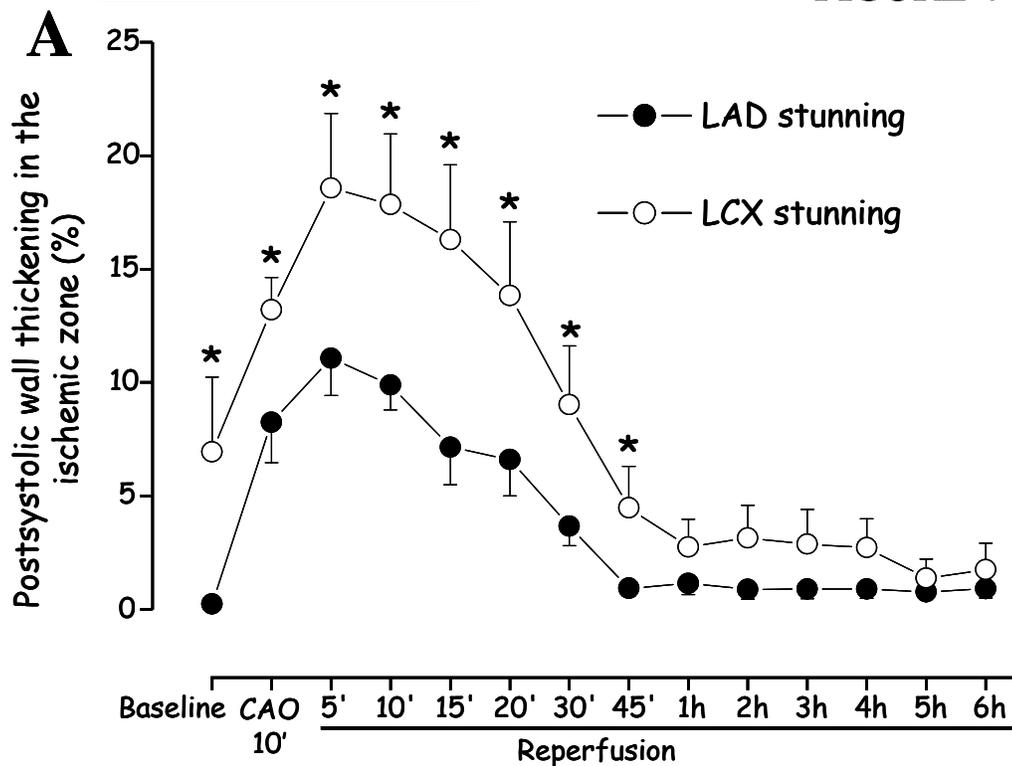


FIGURE 3



Ischemic zone

FIGURE 4



Remote non ischemic zone

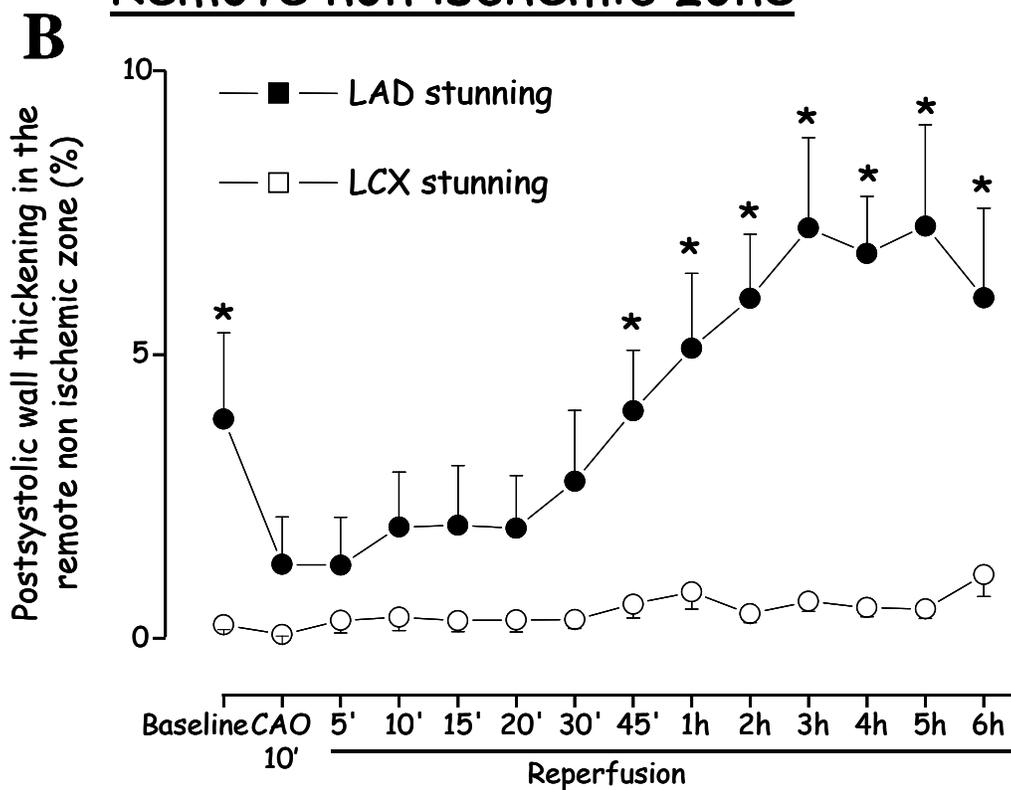
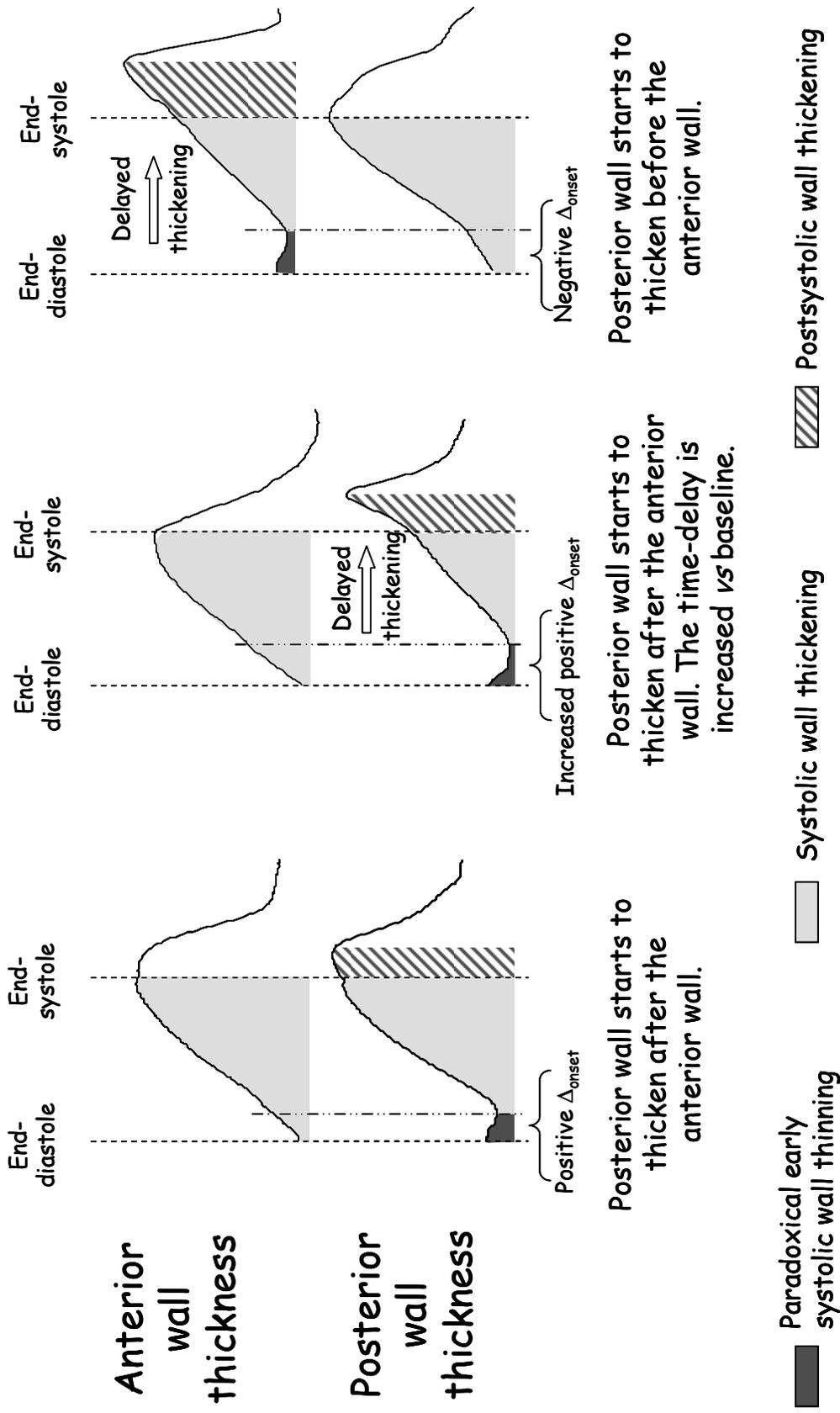


Figure 5

Baseline

LCX stunning

LAD stunning



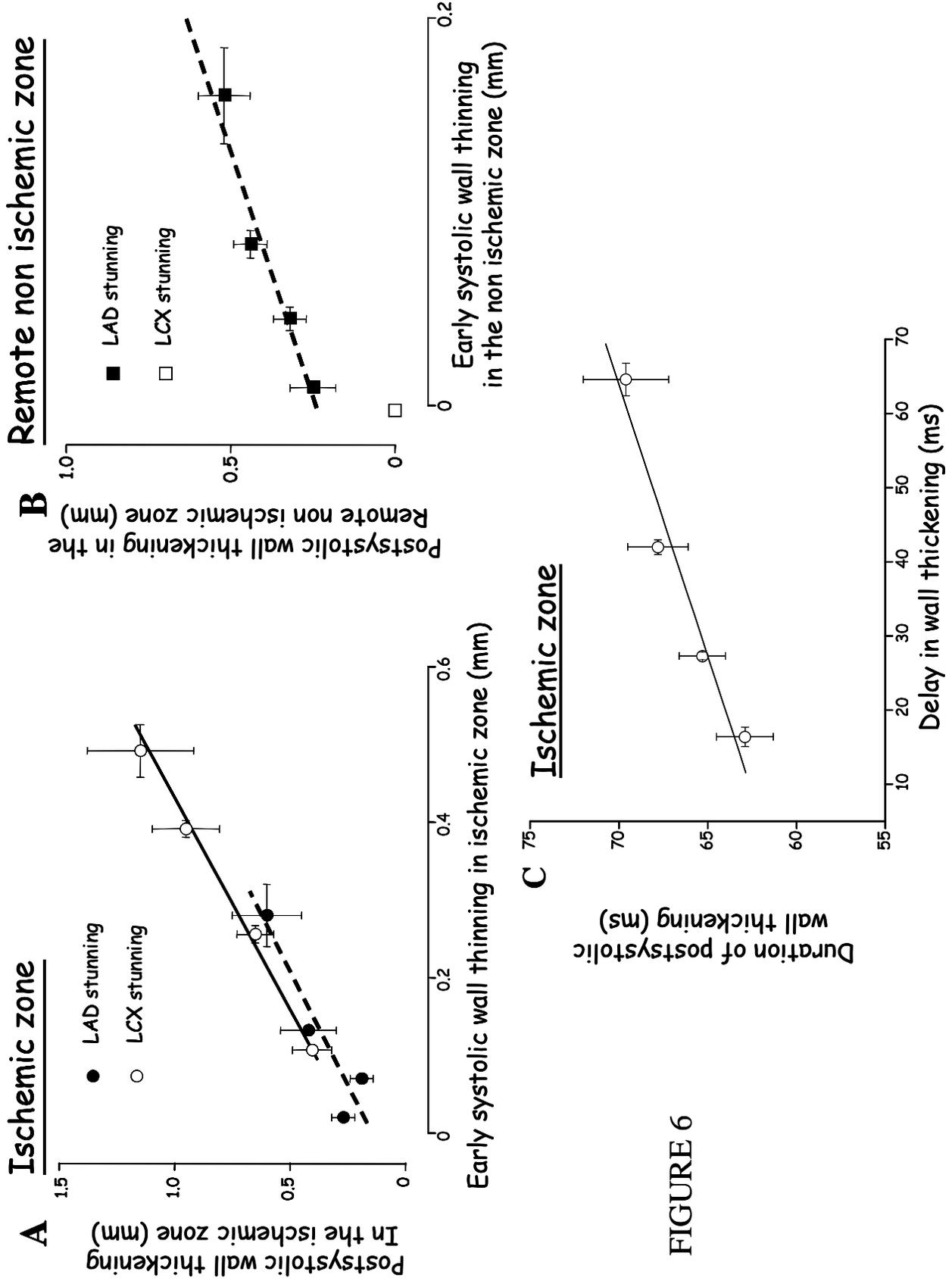


FIGURE 6

FIGURE 7

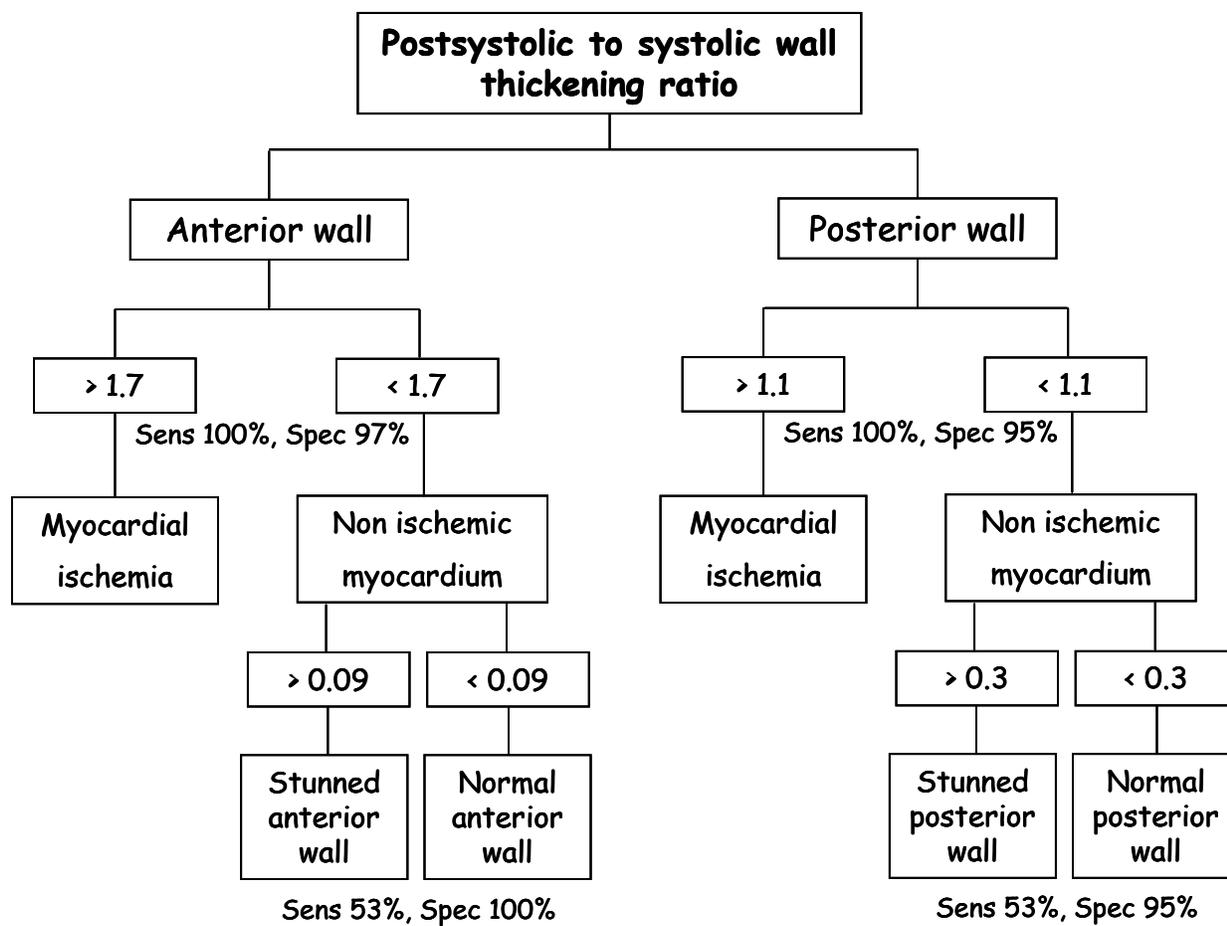


FIGURE 8

TISSUE DOPPLER IMAGING

