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# Preoperative Brain Shift: Study of Three Surgical Cases

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## ABSTRACT

In successful brain tumor surgery, the neurosurgeon's objectives are threefold: (1) reach the target, (2) remove it and (3) preserve eloquent tissue surrounding it. Surgical Planning (SP) consists in identifying optimal access route(s) to the target based on anatomical references and constrained by functional areas. Preoperative images are essential input in Multi-modal Image Guided NeuroSurgery systems (MIGNS) and update of these images, with precision and accuracy, is crucial to approach the anatomical reality in the Operating Room (OR). Intraoperative brain deformation has been previously identified by many research groups and related update of preoperative images has also been studied. We present a study of three surgical cases with tumors accompanied with edema and where corticosteroids were administered and monitored during a preoperative stage [ $t_0, t_1 = t_0 + 10$  days]. In each case we observed a significant change in the Region Of Interest (ROI) and in anatomical references around it. This preoperative brain shift could induce error for localization during intervention (time  $t_S$ ) if the SP is based on the  $t_0$  preoperative images. We computed volume variation, distance maps based on closest point (CP) for different components of the ROI, and displacement of center of mass (CM) of the ROI. The matching between sets of homologous landmarks from  $t_0$  to  $t_1$  was performed by an expert. The estimation of the landmarks displacement showed significant deformations around the ROI (landmarks shifted with mean of  $3.90 \pm 0.92$  mm and maximum of  $5.45$  mm for one case resection). The CM of the ROI moved about  $6.92$  mm for one biopsy. Accordingly, there was a sizable difference between SP based at  $t_0$  vs SP based at  $t_1$ , up to  $7.95$  mm for localization of reference access in one resection case. When compared to the typical MIGNS system accuracy ( $2$  mm), it is recommended that preoperative images be updated within the interval time  $[t_1, t_S[$  in order to minimize the error correspondence between the anatomical reality and the preoperative data. This should help maximize the accuracy of registration between the preoperative images and the patient in the OR.

**Keywords:** Neurosurgical Procedures, Brain Shift, MIGNS, Surgical Workflow.

## 1. INTRODUCTION

This study is set within the context of brain tumor surgery. In this paper, we demonstrate the necessity to update preoperative images in order to allow the recovery of registration error for Multi-modal Image Guided Neurosurgery (MIGNS) systems due to a phenomenon that we call preoperative brain shift. In successful surgery, the neurosurgeon's objectives are threefold: (1) reach the target, (2) remove it and (3) preserve eloquent tissue surrounding it. Surgical Planning (SP) consists in identifying optimal access route(s) to the target based on anatomical references and constrained by functional areas.<sup>1,2</sup> MIGNS systems have been developed and are being used to help reach these objectives. A key component of MIGNS is the accurate registration of preoperative images to the intraoperative coordinate system of the patient.<sup>3</sup> The first registration step consists in a rigid transform, based on assumptions that are not verified during neurosurgical procedures. Intraoperative brain deformation has been previously identified by many research groups and related update of preoperative images

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has also been studied.<sup>4,5</sup> One study<sup>6</sup> has shown that the surface of the brain is deformed by up to 25mm after *skull opening*, which could lead to substantial errors in MIGNS systems. To our knowledge, there is no study that discuss the possible deformations before skull opening. In particular, our study addresses the problem of possible deformations in the case of tumors associated with edema at the preoperative stage. Thus, in this paper we introduce the concept of *preoperative brain shift*.

Tissue **edema** is a pathological condition involving an increase of the amount of fluid in tissue.<sup>7</sup> Brain edema represents a disturbance of the volume equilibrium which must be compensated by a reduction in other fluid and blood compartments. When this compensation is inadequate, tissue pressure and intracranial pressure increase. For standard hospital **protocol**, after the diagnosis, the edema is treated by administration of corticosteroids during the preoperative phase until intervention time and no update of images is requested before the intervention. Let us define  $t_0$  as the time of preoperative image acquisition and  $t_S$  the time of intervention. During  $[t_0; t_S[$ , the patient is administered corticosteroids to regularize the intracerebral pressure and to improve neurological deficit due to edema. Since no imaging is typically performed during this interval, the MIGNS system registration, with 2 mm<sup>8</sup> of accuracy, is based on preoperative images acquired at time  $t_0$ . Our **hypothesis** is that there will be deformations of the ROI induced by corticosteroids administration during preoperative stage  $[t_0; t_S[$ . The edema should shrink, while at the same time the tumor will likely grow. This will induce a significant displacement of neighboring structures over a large region of interest; and to illustrate that point, we present a study of three patients with tumors and severe accompanying edema where corticosteroids were administered and monitored during a preoperative stage  $[t_0, t_1 = t_0 + 10 \text{ days}]$ . Our **objective** is to capture the shift in closed cranium, in these cases where parameters are controlled (tumor localization, edema volume, tumor volume, and corticosteroids administration) without surgical manipulation and mechanical deformation relied to skull opening. To initialize properly the MIGNS systems by correcting the preoperative brain shift implies proper initialization of the well known brain shift phenomenon.

## 2. MATERIAL AND METHODS

### 2.1 Clinical data and images protocol acquisition

The studied cases were three patients with tumors presenting an important surrounding edema: the first patient presented tumor distributed bilaterally with foci in both left and right hemispheres, the second patient revealed right frontal tumor, and the third patient presented ventricular tumor. The treatment consisted in tumor biopsy for the first and third patient, and tumor resection for the second patient. Our imaging protocol included 3T-MR imaging (Philips Medical Systems) using: (1) three-Dimensional (3D) T1-weighted MRI ( $TR = 9.89 \text{ ms}$ ,  $TE = 4.59 \text{ ms}$ , 1 voxel = 1 mm<sup>3</sup>), (2) 3D T1-weighted Gadolinium enhanced ( $TR = 9.89 \text{ ms}$ ,  $TE = 4.59 \text{ ms}$ , 1 voxel  $\simeq$  1 mm<sup>3</sup>) to increase the detection of the tumor and (3) 2D axial T2-weighted Flair ( $TR = 11000 \text{ ms}$ ,  $TE = 125 \text{ ms}$ , resolution :  $0.34 \times 0.34 \times 4 \text{ mm}^3$ ) to maximize information about the edema. In respect to our hypothesis, we set the time  $t_1$  to 10 days after the first preoperative acquisition ( $t_1 = t_0 + 10 \text{ days}$ ).

### 2.2 Image Processing WorkFlow (IPWF)

The IPWF was broken down in two parts: (1) segmentation of the structures in the different MRI sequences; and (2) reformatting of all structures in the same reference frame (T1-weighted at acquisition time  $t_0$ ) for comparison. The IPWF (Figure 1) included:

1. Image preprocessing: we corrected the images intensity inhomogeneities<sup>9</sup> in order to improve the segmentation process. To minimize the impact of noise on the image processing performance, we denoised the images using NL-means algorithm.<sup>10</sup>
2. Image registration: we performed rigid image registration by maximization of the mutual information between the images using the NEWUOA algorithm.<sup>11</sup> We note the matrix of rigid-body registration from sequence  $A$  at  $t_i$  acquisition time to sequence  $B$  at  $t_j$  acquisition time as follow:

$$M_{t_i, t_j}^{A, B}, i, j \in \{0, 1\}, A, B \in \{T1, Gado, Flair\}$$

3. Image segmentation: we segmented the structures of interest (i.e tumor, edema, ventricles, and the brain) on the images by combining manual segmentation using ITK-SNAP<sup>12</sup> and automatic segmentation based on level set method.<sup>13</sup> We noted by  $V_{t_i}^A, i \in \{0, 1\}, A \in \{T1, Gado, Flair\}$  the volume segmented from image sequence  $A$  at time acquisition  $t_i$ .
4. Geometrical transformations of all volumes to the reference frame are noted as following :

$$V_{t_i, t_j}^{A, B} = V_{t_i}^A * M_{t_i, t_i}^{A, B} * M_{t_i, t_j}^{B, B}$$

where  $V_{t_i, t_j}^{A, B}$  is the volume segmented from sequence  $A$  at acquisition time  $t_j$  reformatted to the sequence  $B$  at time  $t_i, i, j \in \{0, 1\}$  and  $A, B \in \{T1, Gado, Flair\}$

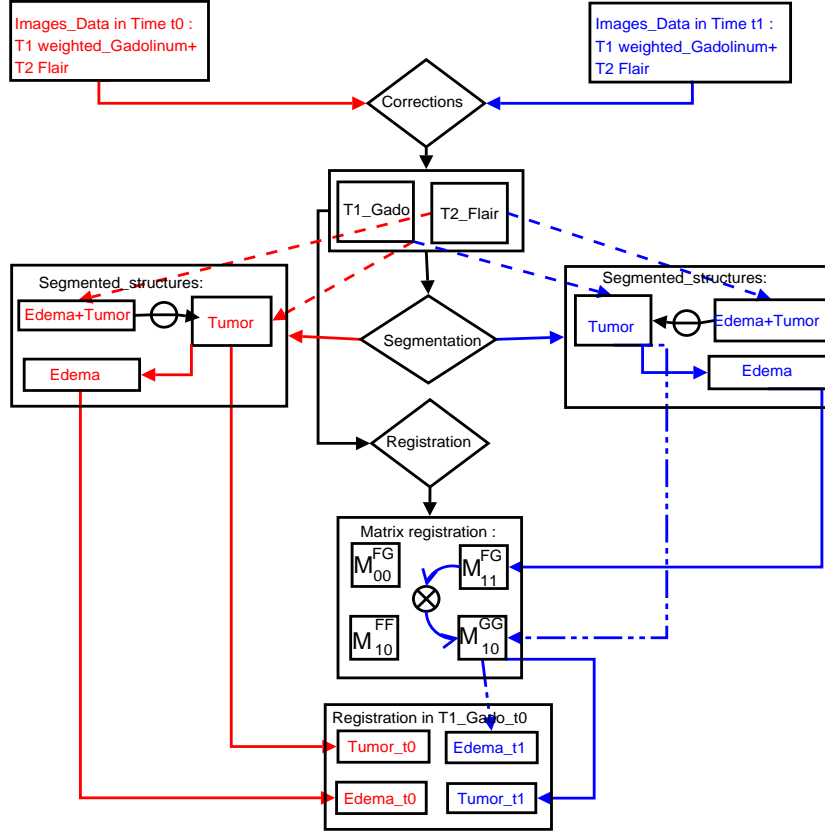


Figure 1. Image processing workflow for volumes segmentation and registration of all volumes in the same reference.

## 2.3 Estimation of local deformations

The estimation of local deformations was divided into three parts : (1) introduction of a metric to evaluate the percentage of volume change and the nature of deformation (shrinking/dilation), (2) estimation of surface deformations of the structures components of the region of interest (ROI), and (3) estimation of the error introduced by the manual segmentation.

### 2.3.1 Shrinking/dilation metric

To estimate the volume change of different structures from acquisition time  $t_0$  to time  $t_1$ , we introduced a local volume change as  $\frac{V_{t_1}}{V_{t_0}}$  and the relative volume change  $\Delta V = \frac{V_{t_1} - V_{t_0}}{V_{t_0}}$ . A positive (negative) value of  $\Delta V$  represents, respectively, an increase (decrease) in the volume. The  $\Delta V$  is a dilation/shrinking metric for results interpretation.

### 2.3.2 Distance maps visualization

To estimate the deformations of the surfaces of the segmented structures and to visualize these deformations according to the localization of the structures, we developed a tool to extract and visualize a signed Distance Maps ( $DM$ ) for the different surfaces. These surfaces correspond, respectively, to the segmented structures at time  $t_0$  (reference structures  $S_{t_0}$ ) and  $t_1$  (target structures  $S_{t_1}$ ).

Without loss of generality, we assumed that  $0 < DSC(S_{t_0}, S_{t_1}) < 1$ , where  $DSC^{14}$  (Dice Similarity Coefficient) measures the spatial overlap between the two segmentations ( $S_{t_0}, S_{t_1}$ ) and is defined as follow:

$$DSC(S_{t_0}, S_{t_1}) = \frac{2(S_{t_0} \cap S_{t_1})}{(S_{t_0} + S_{t_1})}$$

The distance maps visualization was performed as following:

**Initialization:**

1. Take two point sets  $S_{t_0}$  and  $S_{t_1}$
2. Initialize the distance maps  $DM(x, y) = 0 \quad \forall x \in S_{t_0}, \quad y \in S_{t_1}$

**Iterations:**

3. For each point  $x_0 \in S_{t_0}$ , find the closest point  $x_1 \in S_{t_1}$
4. Define the sign of the distance:

$$\text{sign}(DM(x_0, x_1)) = \begin{cases} (-) \text{(i.e shrinking)} & \text{if } x_1 \in \text{Interior}(S_{t_0}), \\ (+) \text{(i.e dilation)} & \text{else} \end{cases}$$

5. Calculation of the distance:

$$DM(x_0, x_1) = \text{sign}(DM(x_0, x_1)) * \|x_1 - x_0\|_2$$

**Visualization:**

6. Display the distance maps for the surfaces  $S_{t_0}$  and  $S_{t_1}$ , with color coding proportional to the distance.

### 2.3.3 Error of manual segmentation and partial volumes effects

The expert\* segmented the tumor twice for one case study at time  $t_0$  and time  $t_1$ . The variation of volume between both segmentations gives an approximation of the manual volume segmentation error. The manual segmentation is performed at voxel level. To evaluate the partial volume effects, the expert displayed one segmentation and delineated the corresponding contour. This 3<sup>rd</sup> segmentation gives a relative volume change according to subvoxel ignorance.

## 2.4 Estimation of regional displacements

### 2.4.1 Landmarks displacement around the ROI

To quantify displacement of neighboring structures to the ROI, the expert identified eight anatomically homologous landmarks  $L_{t_i}^k, i \in \{0, 1\}, k \in \{0, ..8\}$  using MINC tools<sup>†</sup>. We note  $L_{01}^k = (L_{t_0}^k, L_{t_1}^k)$  the matching couple between landmark  $L_{t_0}^k$  at time  $t_0$  and the corresponding landmark  $L_{t_1}^k$  at  $t_1$ . We note by  $\|L_{01}^k\|_2 = \|(L_{t_0}^k, L_{t_1}^k)\|_2$  the Euclidean distance between each  $k^{th}$  landmark at time  $t_0$  and the  $k^{th}$  corresponding landmark at time  $t_1$ .

### 2.4.2 Reference landmarks displacement vs registration

To validate the precision of landmarks identification according to the error of rigid-body registration used in the image processing Workflow, the expert selected eight additional landmarks that are not supposed to be deformed (e.g the nasion, the eyes). We note this set of reference landmarks  $F_{t_i}^k, i \in \{0, 1\}, k \in \{0, ..8\}$ . The registration was accepted if the mean of displacement of the different reference landmarks was less than 1mm.

\*Neurosurgeon, neuroanatomist expert (X.M.)

<sup>†</sup><http://www.bic.mni.mcgill.ca/software/>

## 2.5 Estimation of ROI components displacement: Center of mass displacement

We supposed that the displacement of the ROI components (Tumor, Edema) can be characterized by the movement of their center of mass. We defined center of mass for each volume  $V$  of ROI components ( $CM(V)$ ) and we note  $\|(CM(V_{t_0}), CM(V_{t_1}))\|_2$  the Euclidean distance between the volume  $V_{t_0}$  at acquisition time  $t_0$  and the volume  $V_{t_1}$  at acquisition time  $t_1$ .

## 2.6 Introduction of Surgical Planning (SP) Error

For each intervention, the SP contribution consists of two parts : (1) localization of the target, and (2) definition of a road map according to the anatomical references (cortical gyri or sulci) and constraints (functional areas). We defined the difference between SP based on the acquisition time  $t_0$  ( $SP_{t_0}$ ) and SP based on  $t_1$  time ( $SP_{t_1}$ ) by given couple of errors related to: (1) localization of targets (ROI) from  $t_0$  to  $t_1$  and (2) displacement of anatomical references (like cortical gyri or sulci) from  $t_0$  to  $t_1$ . If we classify the data according to the treatment, we can define the error as follow :

$$Error(SP_{t_0}, SP_{t_1}) = \begin{cases} [\|(target_{t_0}, target_{t_1})\|_2; \|(sulci_{t_0}, sulci_{t_1})\|_2] & \text{if resection,} \\ [\|(target_{t_0}, target_{t_1})\|_2; Mean(landmarks displacement)] & \text{if biopsy.} \end{cases}$$

Where :  $target_{t_0}, target_{t_1}$  are the targets (tumors for our three surgical cases) from acquisition time  $t_0, t_1$  respectively and  $sulci_{t_0}, sulci_{t_1}$  are the sulci from  $t_0, t_1$ .

## 3. RESULTS

### 3.1 Estimation of local deformations

#### 3.1.1 Local volume changes

From Table 1, a significant increase in the tumor volumes for the first and the third patient contrasts with decrease of tumor volume for the second patient. However, the edema and the global ROI (edema + tumor) volumes decreased for all patients by at least 12.18%. The variation of volume of ventricles depends on tumor localization. We observe for the second patient a significant increase (+21.77%).

Table 1. Table representing volume changes  $\Delta V$  for the three patients

Structures / patient	Volume changes $\Delta V = \frac{V_1 - V_0}{V_0} \%$		
	1 <sup>st</sup> patient	2 <sup>nd</sup> patient	3 <sup>rd</sup> patient
Brain	-4.92%	+1.64%	+2.01%
Tumor	+60%	-28.60%	+16.58%
Edema	-32.92%	-31.00%	-15.34%
ROI=Edema+Tumor	-13.62%	-30.74%	-12.18%
Ventricles	-0.94%	+21.77%	-13.87%

#### 3.1.2 Manual segmentation error

Table 2 shows, for the second patient, a non significant partial volume effects due to the manual segmentation by the expert. We observed for the two segmentations of the tumor from time  $t_1$  a variation:  $\Delta S_{Tumor} = -0.407\%$ . Comparing to the volume changes of the tumor for the second patient (Table 1), we observed:

$$\Delta S_{Tumor} = -0.407\% \ll -28.60\% = \Delta V_{Tumor}$$

#### 3.1.3 Distance maps visualization

From Figure 2, we distinguished the shrinking/dilation of different surfaces of structures from time acquisition  $t_0$  to time  $t_1$ . The visualization of these distance maps shown location of the shrinking or dilation and illustrates significant deformations of surfaces and confirmed the results of volume changes. The visualization of brain distance map from  $t_0$  to  $t_1$  merged with ROI localization shows a shift of the brain according to the shrinking/dilation of the structures component of the ROI.

Table 2. Error of manual volume segmentations for tumor (2<sup>nd</sup> patient)

	Volumes for tumor segmentation at $t_0$ and $t_1$				
	$S1(mm^3)$	$S2(mm^3)$	$\Delta S_{Tumor} = \frac{S2-S1}{S1}$	$S3(mm^3)$	$\Delta S = \frac{S3-S2}{S2}$
Time $t_0$	17524	16995	-0.03018	17144	0.00876
Time $t_1$	12512	12461	-0.00407	12102	-0.02880

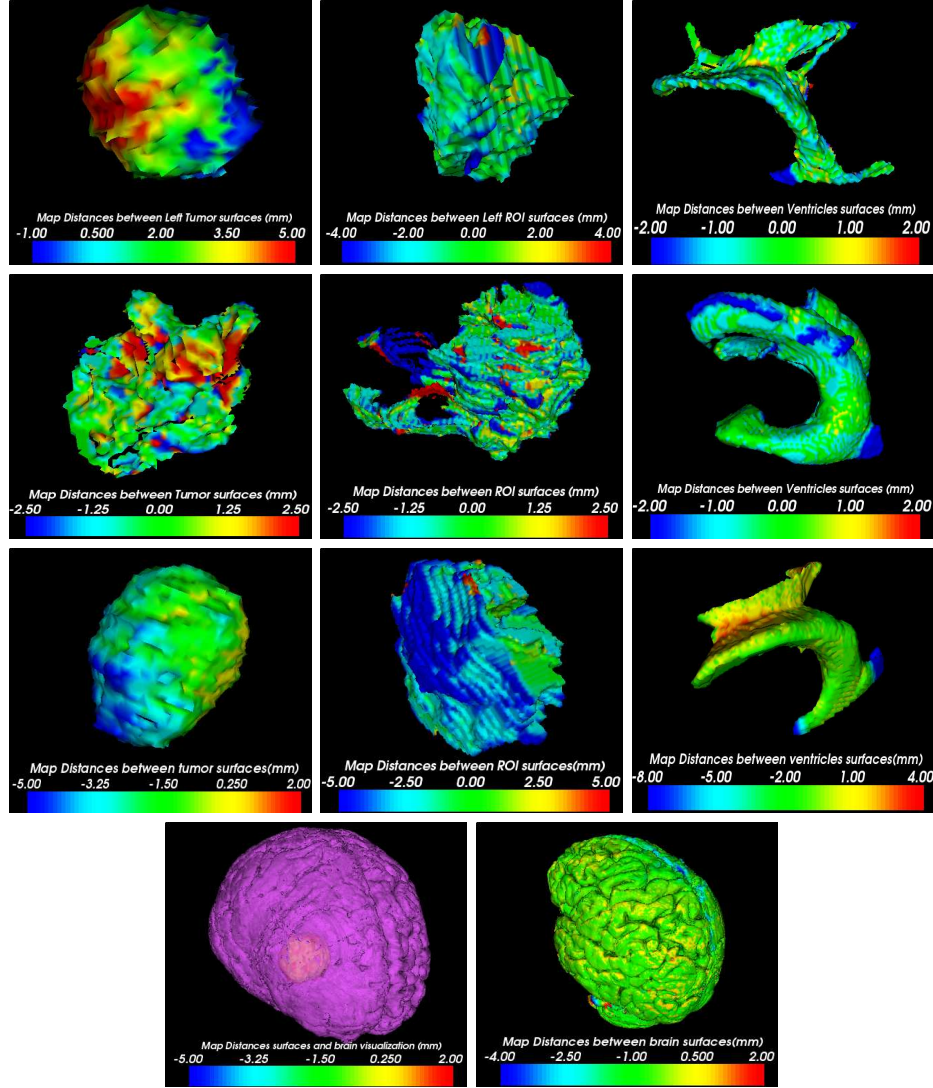


Figure 2. Signed distance maps, based on closest points algorithm, from reference time  $t_0$  to targeted time  $t_1$ . From left to right, distance maps for tumor, ROI(Edema+Tumor), and ventricles. From top to bottom, the three rows correspond to the 1<sup>st</sup>, 3<sup>rd</sup>, and 2<sup>nd</sup> patient respectively. The last row represents for the 2<sup>nd</sup> patient the merging between the tumor localization and the brain distance map.

### 3.2 Estimation of regional displacement

Table 3 shows a significant displacement of landmarks around the ROI of the three patients. For the 2<sup>nd</sup> patient, the mean of displacement was about  $3.90 \pm 0.92$  mm with maximal displacement of 5.45 mm. In second part, the table shows that the rigid registration applied for our IPWF was accepted. For the three patients, the means were:  $0.54 \pm 0.31$  mm,  $0.63 \pm 0.30$  mm, and  $0.83 \pm 0.22$  mm respectively. The mean of distances between matching reference landmarks was inferior to 1 mm.

Table 3. Euclidean distance  $\|\cdot\|_2$  between each landmark  $L_{t_0}^k$  at time  $t_0$  and the corresponding landmark  $L_{t_1}^k$  at time  $t_1$  for the three patients.

		Displacement of Landmarks around the ROI								
Patient/ $\ \cdot\ _2$ (mm)	$L_{01}^1$	$L_{01}^2$	$L_{01}^3$	$L_{01}^4$	$L_{01}^5$	$L_{01}^6$	$L_{01}^7$	$L_{01}^8$	$\mu$	$\sigma$
1 <sup>st</sup> patient	2.14	0.84	1.17	2.36	1.87	1.09	0.89	2.77	1.64	0.69
2 <sup>nd</sup> patient	2.08	3.07	4.17	4.13	4.36	4.25	3.68	5.45	3.90	0.92
3 <sup>rd</sup> patient	2.16	1.47	1.78	2.47	1.73	2.65	1.87	2.89	2.13	0.46
		Displacement of reference landmarks								
Patient/ $\ \cdot\ _2$ (mm)	$F_{01}^1$	$F_{01}^2$	$F_{01}^3$	$F_{01}^4$	$F_{01}^5$	$F_{01}^6$	$F_{01}^7$	$F_{01}^8$	$\mu$	$\sigma$
1 <sup>st</sup> patient	0.17	0.25	1.15	0.63	0.43	0.93	0.44	0.34	0.54	0.31
2 <sup>nd</sup> patient	0.37	0.30	0.43	0.72	1.27	0.89	0.49	0.61	0.63	0.30
3 <sup>rd</sup> patient	0.93	1.19	0.66	0.78	0.87	0.40	0.80	1.01	0.83	0.22

### 3.3 Estimation of ROI component displacement

From (Table 4) we observed a significant displacement of mass center of the ROI (CM(ROI)); for the 3<sup>rd</sup> patient, the CM(edema+tumor) moved by 6.92 mm and for the 1<sup>st</sup> patient, the center of mass of tumor moved by 4.05 mm. These results coupled with landmarks displacement demonstrate first sizable difference between SP based  $t_0$  vs SP based  $t_1$ .

Table 4. The displacement of Center of Mass (CM) for the tumor and the global ROI (Edema+Tumor)

		CM displacement of The ROI components	
Patient/ $\ \cdot\ _2$ (mm)	CM(Tumor)	CM(ROI)	
1 <sup>st</sup> patient	4.052	1.713	
2 <sup>nd</sup> patient	2.706	1.45	
3 <sup>rd</sup> patient	1.971	6.920	

### 3.4 Surgical Planning (SP) Error

For the second patient, the surgeon defined an optimal sulci, to reach the target, for the planning  $SP_{t_0}$  and the corresponding sulci for the planning  $SP_{t_1}$ . The left part of the (Figure 3) shows the difference between the sulci extraction based on time  $t_0$  (yellow color) and the extraction based on time  $t_1$  (blue color). The right part of the (Figure 3) shows the optimal reference sulci to access to the tumor based on  $SP_{t_0}$  (yellow) and the corresponding one according to  $SP_{t_1}$  (blue color). The Euclidean distance between the center of mass of the sulci from  $t_0$  to  $t_1$  was  $\|(sulci_{t_0}, sulci_{t_1})\|_2 = 7.95$  mm and from (Table 3), we note  $\|(tumor_{t_0}, tumor_{t_1})\|_2 = 2.70$  mm. It gives a surgical planning error for the second patient as:

$$Error(SP_{t_0}, SP_{t_1}) = [2.70; 7.95]mm$$

We resume in Table 5 the corresponding errors due to planning based on  $t_0$  vs planning based on  $t_1$  for the three patients.

Table 5. Surgical planning error for the three patients

		Surgical planning error		
	1 <sup>st</sup> patient	2 <sup>nd</sup> patient	3 <sup>rd</sup> patient	
Error( $SP_{t_0}, SP_{t_1}$ )mm	[4.05; 1.64]	[2.70; 7.95]	[1.97; 2.13]	



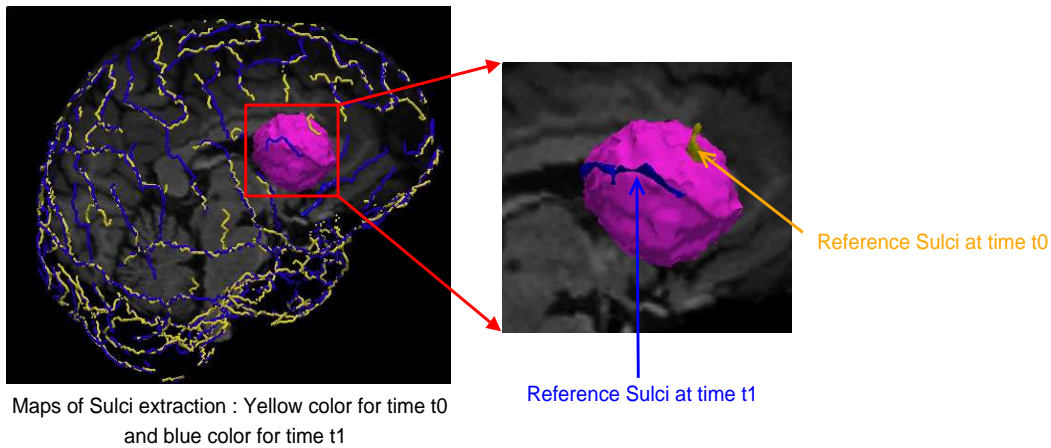


Figure 3. The extraction of sulci based on time  $t_0$  with optimal reference sulci (yellow color) and the extraction based on time  $t_1$  (blue color) with optimal reference sulci to access to the tumor.

#### 4. CONCLUSION AND DISCUSSION

Different studies have focused on compensating the brain shift phenomenon and to correct deformation in intra-operative stage.<sup>5,15</sup> Since temporal aspect is a key factor during neurosurgery, to extract an information about deformation can increase the accuracy of the MIGNS systems. Different parameters related to the phenomenon increase the complexity of the event. Drug responses, gravity, edema and surgical manipulation complicate the understanding of the deformation.<sup>4,16</sup> The brain shift phenomenon is certainly related to the disturbance of the volume equilibrium and a studies<sup>5,17</sup> have shown a cortical brain surface shift of 10 *mm* on average, during surgery and along direction of deformations, after skull opening.

In this study, we addressed another aspect of anatomical deformation related to brain shift in the preoperative phase that we call *preoperative brain shift*. This preoperative brain shift was restricted to the anatomical brain deformations in closed-cranium. We hypothesized, for our data set of patients (three surgical cases), that the presence of edema and tumor creates a mass effect and that after corticosteroids administration during stage  $[t_0, t_1]$ , both the shrinking of edema and growth of tumor induce lack of tissue and provide displacement of neighboring structures of the ROI. The three surgical cases illustrate the existence of the preoperative brain shift and initialize preliminary measures to understand the shift in closed cranium under controlled parameters (tumor localization, edema volume, tumor volume, and corticosteroids administration) without surgical manipulation. The signed distance maps introduced in this study can be used for understanding and modeling preoperative deformation. According to brain surface deformations, we will be able to localize an optimal craniotomy in order to minimize the shift due to the decrease of intracranial pressure after skull opening. The local volume changes of the components of the ROI can be related to the localization of these components; the significant increase of the volume of ventricles for the second patient (Table 1) can be explained by the fact that the tumor and the edema are inside the ventricles.

On the methodological side, our study suffers from three principal points: (1) rigid body registration, (2) manual segmentation, and (3) intra-expert variability in landmarks identification. For further work, we will introduce elastic body registration to extract the deformation field and to identify the features for direction of deformation. For manual segmentation by the expert, we observed that we can ignore the partial volume effects comparing to the significant volume changes, but we have to introduce the error related to different experts. For homologous landmarks identification, we have to estimate the displacement errors associated with placement of the landmarks and errors of locating the fiducial points due to the intra-expert variability. Another further step of our work will be to propose a realistic model of tumor growth, that is in general difficult,<sup>18</sup> and combine it with model of edema shrinking in order to build a first model for preoperative brain shift.

Further analysis, with more clinical cases, will certainly emphasize a new surgical workflow that determine a time  $t_1 \in [t_0, t_S[$  ( $t_S$  time of intervention), respecting clinical temporal constraints and processing time of images

(preprocessing, fusion and segmentation), after which new preoperative imaging must be performed in order to initialize properly the MIGNS systems and recover the error of misregistration. In fine, this would be a proper initialization of the intraoperative brain deformation and help approach the reality in the operating room.

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